






1 CirculationModels.jl - A ModelingToolkit Library for 2 0D-Lumped-Parameter Models of the Cardiovascular 3 Circulation

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8 Summary

9 Within the realm of circulatory mechanics, lumped parameter (0D) modelling ([Shi et al., 2011](#))
10 offers the unique ability to examine both cardiac function and global hemodynamics within
11 the context of a single model. Due to the interconnected nature of the cardiovascular system,
12 being able to quantify both is crucial for the effective prediction and diagnosis of cardiovascular
13 diseases. Lumped parameter modelling derives one of its main strengths from the minimal
14 computation time required to solve ODEs and algebraic equations. Furthermore, the relatively
15 simple structure of the model allows most personalized simulations to be automated. Meaning
16 the ability to embed these lumped parameter models into a clinical workflow could one day
17 become trivial ([Bozkurt et al., 2022](#); [Holmes & Lumens, 2018](#)).

18 *CirculationModels.jl* is a [Julia](#) ([Bezanson et al., 2017](#)) package, built on the acausal modelling
19 framework provided by *ModelingToolkit.jl* ([Ma et al., 2021](#)), containing all the common
20 elements plus more needed for effective and realistic lumped parameter modelling. Currently
21 *CirculationModels.jl* supports common elements such as a capacitor, resistor, inductance and
22 diodes ([Nicolaas Westerhof et al., 2010](#)), which act as simple valve functions. We also make
23 extensions to the common elements to include constant compliance chambers, non-linear and
24 Poiseuille resistances ([Pfitzner, 1976](#)). Plus the Double-Hill, and Shi activation functions which
25 are used as the cardiac driving chamber elastance's ([Korakianitis & Shi, 2006](#); [Stergiopoulos
26 et al., 1996](#)). We also include non-linear valve functions from Shi, and Mynard ([Korakianitis
27 & Shi, 2006](#); [Mynard et al., 2012](#)). Alongside individual components we also have created
28 a collection of sub compartments including, full circulatory, systemic, pulmonary and heart
29 models. We then also break down these full systems into collections of elements such as the
30 famous Windkessel models ([Nico Westerhof et al., 2009](#)) to give the user full control over their
31 modelling.

32 Users can easily add new elements to *CirculationModels.jl* using *ModelingToolkit.jl* functions.

33 Statement of need

34 Lumped parameter modelling has become an essential part of contributing strongly to our
35 understanding of circulatory physiology. Lumped parameter models have been used in many
36 different contexts across cardiovascular medicine such as aortic valve stenosis, neonatal
37 physiology and detection of coronary artery disease ([Dash et al., 2022](#); [Laubscher et al., 2022](#);
38 [Sepúlveda Oviedo et al., 2022](#)). There already exists some popular packages within both
39 Simulink and Modelica such as the “Cardiovascular library for lumped-parameter modeling”
40 ([Rosalia et al., 2021](#)) and “Physiolibrary” ([Mateják et al., 2014](#)) respectively. These languages

41 operate a block orientated “drag and drop” approach with Modelica been the common choice
42 due to it’s acausal modelling approach (Schweiger et al., 2020). Other languages, based on
43 XML, exist for lumped parameter modelling such as CellML (Cuellar et al., 2003) and SBML
44 (Hucka et al., 2003), while these are great for exchanging models they are often difficult
45 to implement and model analysis is limited. A common theme within all current lumped
46 parameter modelling software is the systems inability to deal with complex event handling and
47 non-linear components. Being based on *ModelingToolkit.jl*, *CirculationModels.jl* overcomes
48 these limitations by leveraging the wider *SciML* framework.

49 *CirculationModels.jl* provides the Julia community with a quick and effective way to perform
50 lumped parameter modelling, being the first within the field to leverage both multiple dispatch
51 and JIT compilation. As a result of Julia’s architecture, as the complexity of the model
52 increases the model analysis time does not become unreasonable.

53 Other packages exist which allow users to import models from other frameworks, CellML-
54 Toolkit.jl (Iravanian & others, 2021) and OpenModelica.jl (Tinnerholm et al., 2022). *Circu-*
55 *lationModels.jl* goes beyond these by providing a lumped parameter modelling library with
56 seamless integration with the SciML framework (Dixit & Rackauckas, 2022; Rackauckas et al.,
57 2020; Rackauckas & Nie, 2017) which allows for extensive and efficient model analysis. Since
58 both the modelling library and the framework it is built on are pure Julia, new components
59 can be developed in a transparent and consistent manner.

60 Using Julia, *CirculationModels.jl* models compute significantly faster than models implemented
61 in Matlab or Python, and at the same speed as specialised C-code (Table 1). This allows the
62 models to run in real-time, and opens the possibility of global parameter optimisation, global
63 sensitivity analysis.

64 The modular, acausal approach also allows quick and straightforward changes to the topology
65 of the model, which can be automated using meta-programming techniques.

66 Example

67 Validation and benchmarking was performed on a full, 4-chamber, model of the circulation
68 system proposed by (Korakianitis & Shi, 2006) (Figure 1). This model was previously imple-
69 mented in CellML (Shi et al., 2018), which makes it an ideal candidate for validation of the
70 new modeling library¹.

71 Model results from *CirculationModels.jl* model (Figure 2) are a perfect match for the CellML
72 model. The CellML model was run in three versions: (1) imported into *ModelingToolkit.jl* using
73 *CellMLToolKit.jl*, (2) Matlab code exported from CellML, (3) Python/SciPy code exported
74 from CellML. Speedup against Matlab and Python is 2 and 3 orders of magnitude, respectively
75 (Table 1).

¹Note that CellML does not allow the callbacks which are required for the extended valve model, so only the simplified model can be compared. The *CirculationModels.jl* implementation of (Korakianitis & Shi, 2006) includes the extended model as well.

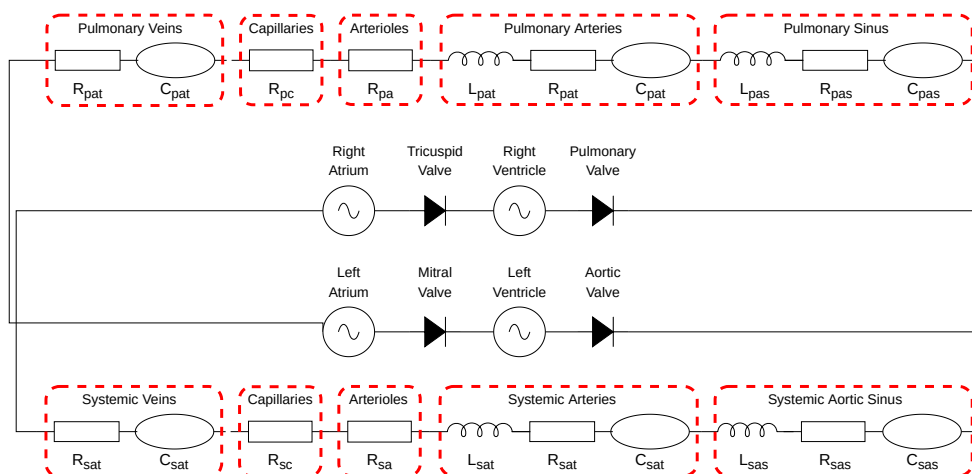


Figure 1: 4-chamber, full-circulation model from (Korakianitis & Shi, 2006). Groupings in dashed rectangles are implemented as compound subsystems, which in turn have been composed from individual resistor, compliance, and inductance elements. Ventricles and Atria implemented as time-variable elastances. Both simplified and dynamic, non-linear valve models are implemented.

Table 1: Simulation time comparison for a single run of (Korakianitis & Shi, 2006). CirculationModels.jl model was implemented from scratch. CellML model was imported into ModelingToolkit.jl using CellMLToolkit.jl, Matlab and Python models were created from the CellML code and downloaded from the CellML Model Repository.

CirculationModels.jl	CellMLToolkit.jl	Matlab (ode45)	Python (scipy.solve)
1x	1.6x	272x	963x

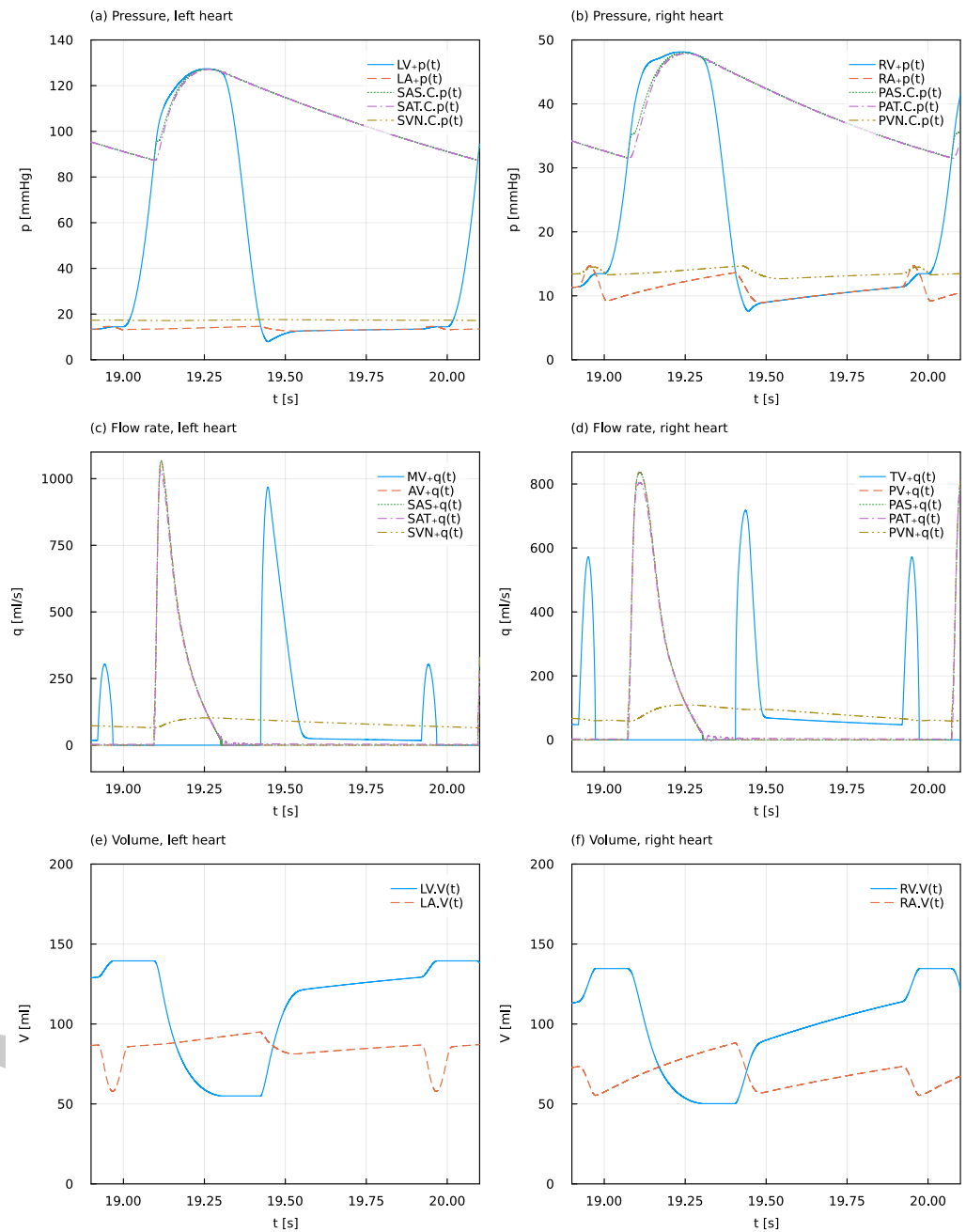


Figure 2: (a-f) Results for simplified model (Korakianitis & Shi, 2006) implemented in *CirculationModels.jl*. These results match the results from the CellML models (not shown).

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